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**Basics of Image Processing**

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Leiden University Medical Center  
Delft University of Technology

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**New 3 year education programme**

- Year 1: Image Segmentation
  - Methodology
  - Validation
- Year 2: Image registration and dynamic analysis
  - Methodology
  - Applications
  - Tracking
- Year 3: Quantitative imaging biomarkers (QIB)
  - Basics
  - QIB in neurological disease
  - QIB in cardiovascular disease

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**Image segmentation**



- Introduction
- Image segmentation approaches
  - Pixel/voxel classification
  - Deformable model based segmentation
  - Active shape and appearance models
  - Atlas-based segmentation
- Validation and challenges

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**Introduction**

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**Non-invasive imaging**

Röntgen' lab

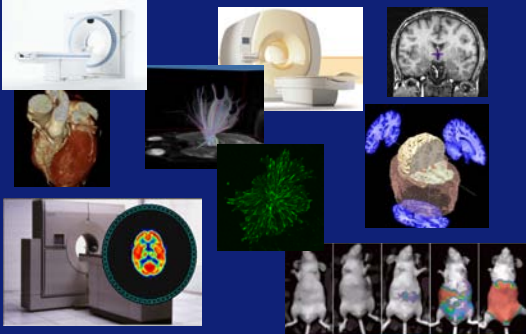


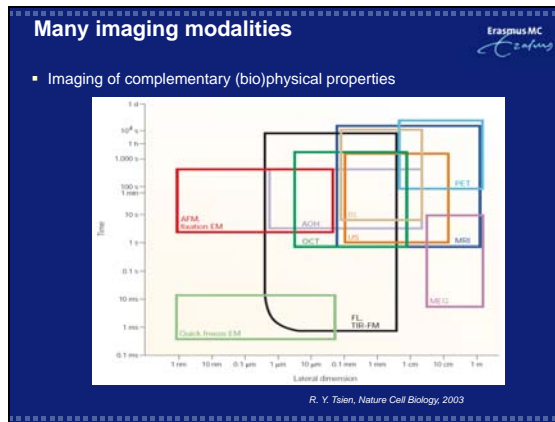
22 dec, 1895

Wilhelm Conrad Röntgen  
Discovery X-rays, 8 november 1895  
First Nobel prize in Physics: 1901

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**We see brains "think", hearts beat, and follow processes to the molecular level**





### Challenges

- Size and complexity of imaging data
- Multiple imaging modalities
- Multiple time points

➡ Data Explosion

How to enable

- Integrated visualization
- Quantitative image analysis
- Objectivity and reproducibility
- Full exploitation of available information
- Development of imaging biomarkers

➡ Automation

### Computing tasks

- Image registration
- Image segmentation
- Tracking and motion analysis
- Quantitative image analysis
- Image visualization and fusion

### Computing tasks

- Image registration
- Image segmentation**
- Tracking and motion analysis
- Quantitative image analysis
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### Segmentation

- Define objects in a dataset in order to
  - distinguish relevant and irrelevant data
  - quantitative measurements
  - visualization

by

- manual outlining
- simple algorithms (thresholding)
- advanced (semi-)automated algorithms

### Segmentation techniques

- "Low level"
  - Pixel/voxel classification**
    - Using intensities, gradients, texture
    - Grouping
- Model based
  - Including prior knowledge
    - Restricted parameterization
      - Imposed: **Deformable models**
      - Learned: **Active shape/appearance models**
      - Atlas-based segmentation**

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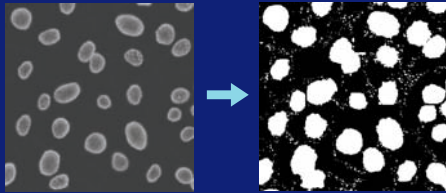
**Pixel classification**

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**Simple example: thresholding**

- Separating relevant structures from irrelevant background

Example of thresholding:



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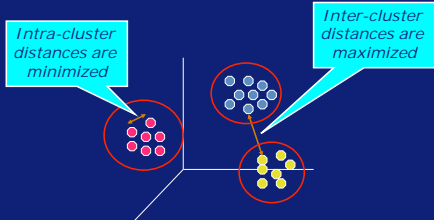
**Supervised classification versus unsupervised clustering**

- Unsupervised clustering
  - Group similar pixels together to form clusters
    - Minimize intra-class distance
    - Maximize inter-class distance
- Supervised classification:
  - Class label is available for training samples
    - Build model from training data
    - Predict voxel label unseen data using model

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**What is clustering?**

- Form clusters of voxels such that they are similar (or related) to each other and different from voxels in other clusters



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**Overview of K-Means Clustering**

- K-Means is a partitional clustering algorithm based on iterative relocation that partitions a dataset into  $K$  clusters.

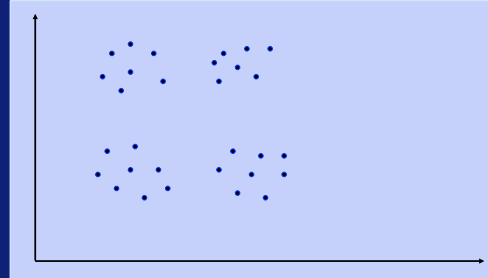
**Algorithm:**

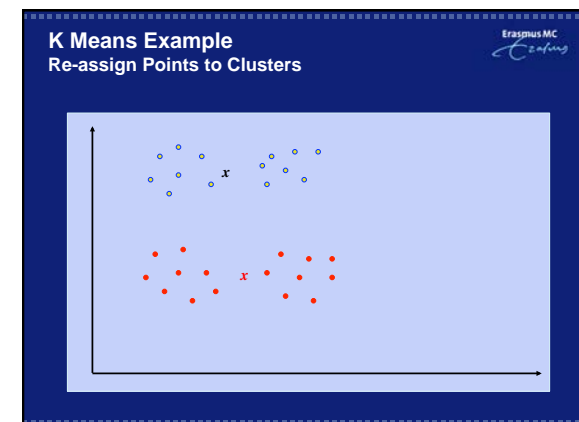
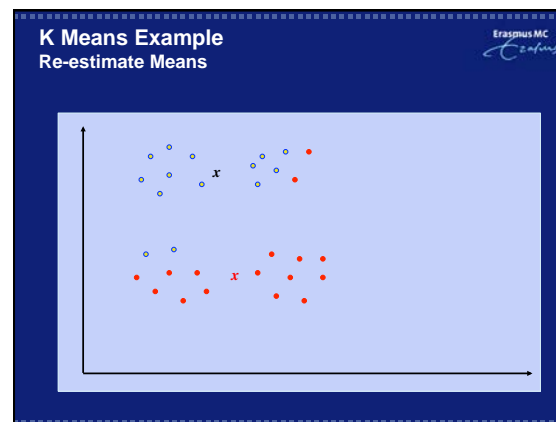
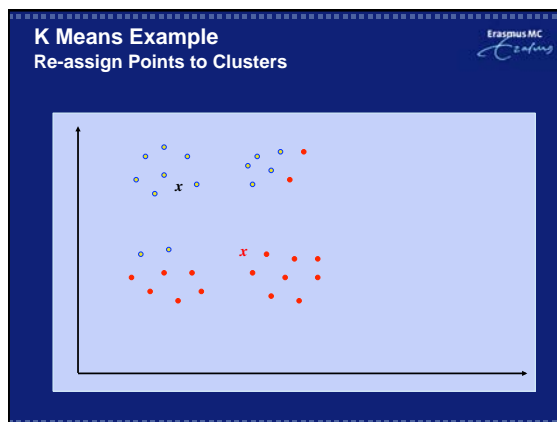
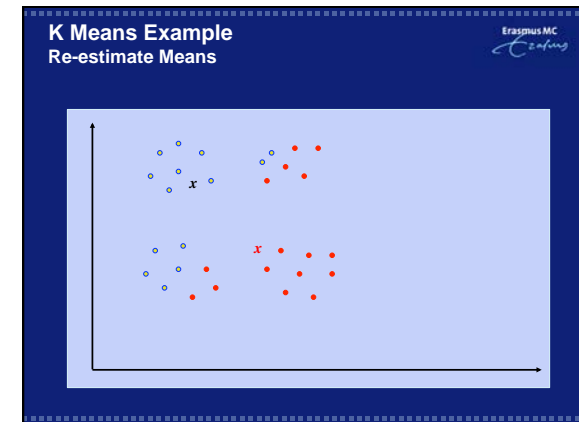
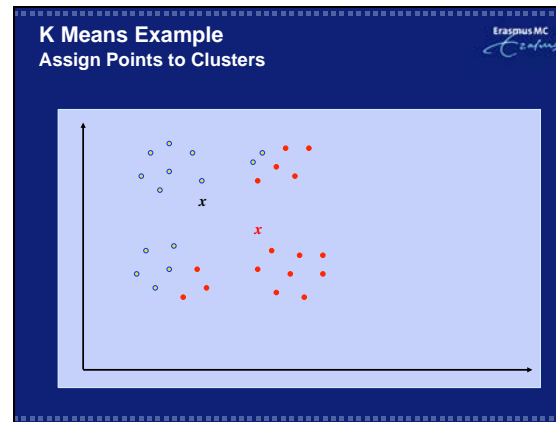
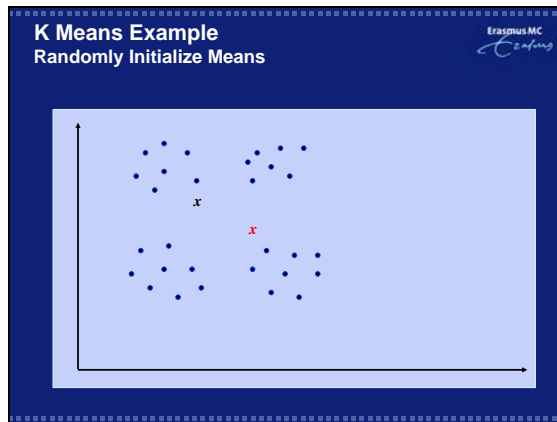
Initialize  $K$  cluster centers randomly. Repeat until *convergence*:

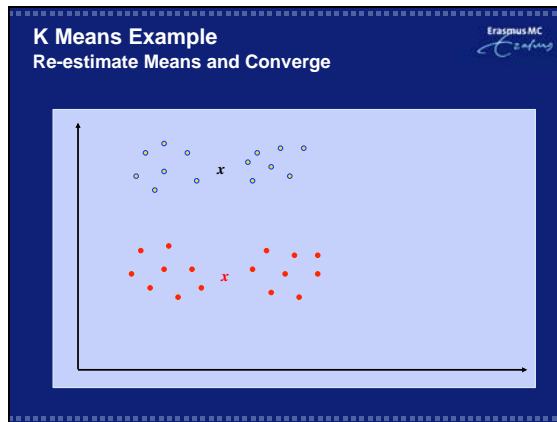
- **Cluster Assignment Step:** Assign each data point to the nearest cluster
- **Center Re-estimation Step:** Re-estimate each cluster center as the mean of the points in that cluster

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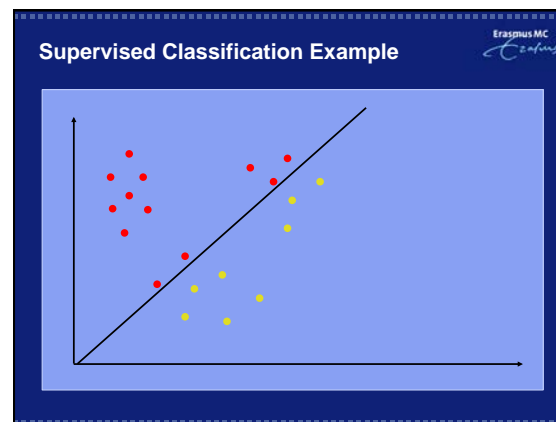
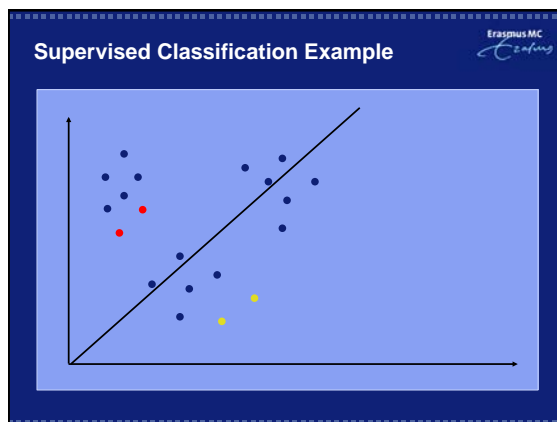
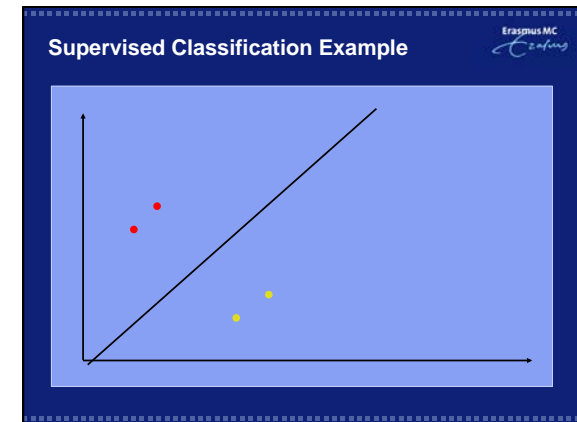
**K Means Example**







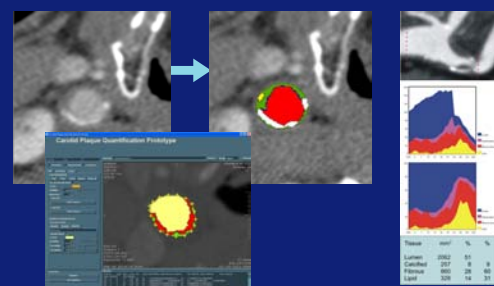
- ### Many clustering algorithms
- K-Means
  - Hierarchical clustering
  - Graph based clustering (Spectral clustering)
  - Bi-clustering



- ### Classification algorithms
- K-Nearest-Neighbor classifiers
  - Naïve Bayes classifier
  - Linear Discriminant Analysis (LDA)
  - Support Vector Machines (SVM)
  - Logistic Regression
  - Neural Networks

## Quantification of atherosclerotic plaque

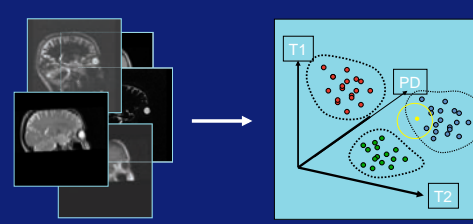
- Hounsfield unit based definition of plaque composition



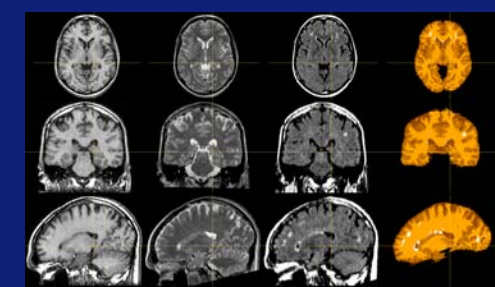
Tissue	min	max	%
Lumen	-1000	-50	10
Calcified	130	300	15
Fibrous	30	130	40
Lipid	-100	30	35

## Automated tissue segmentation


- Determining GM, WM, CSF volume as a function of age
- kNN based, with automated training



## Automated segmentation grey/white matter, CSF, WML





## Deformable model based segmentation




## Snakes

- Introduced in 1988 (Kass, Terzopoulos, Witkin)
- Idea: a curve is fitted iteratively to the data based on
  - Image data
  - Curve shape until convergence
- "Active contour", "deformable model"
- In 3D surfaces

## Example: Euclidean shortening flow

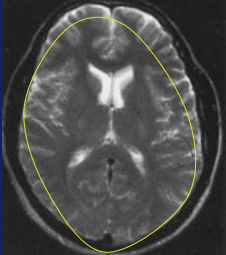



$$\frac{\partial C}{\partial t} = g(\kappa) \vec{N}$$

$$(g = \kappa)$$

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### Geodesics: shortest paths on a manifold

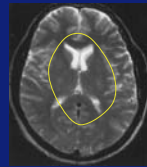
$$E(u) = \int_0^1 F(u, u_x) dx$$

$$u(0) = (a); u(1) = (b)$$

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### Snakes

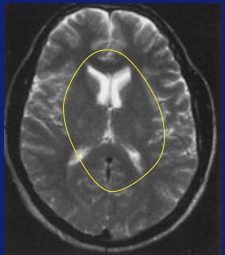
$$C(s) = (x(s), y(s))$$

$$E = \int_0^1 [E_{\text{int}}(C(s)) + E_{\text{ext}}(C(s))] ds$$


- $E_{\text{int}}$  is the internal energy at all points of the snake
- $E_{\text{ext}}$  is the external energy formed by the external forces attracting the curve
- Objective: Find the curve that minimizes the energy functional

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### Snake energy



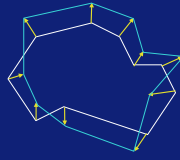
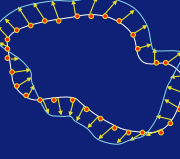
$$E_{\text{int}} = \omega_1 |C'(s)|^2 + \omega_2 |C''(s)|^2$$

$$E_{\text{ext}} = -\|\nabla I\|^2$$

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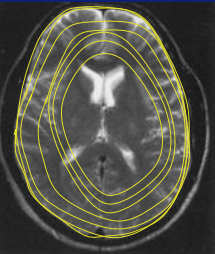
### Representations

- Parametric active contour
  - Stored as vertices
  - Each vertex is moved iteratively
- Geometric active contour
  - Parameterization
  - Sampled at each iteration
  - Each sample is moved
  - New coefficients are computed (interpolation)

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### Snake algorithm





- For all points in snake
  - Sample a number of locations in the neighborhood
  - Select location with minimal energy
  - Repeat until convergence

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### Carotid imaging and analysis in 3D

- Automated artery segmentation and quantification

Better accuracy and reproducibility

## Snake advantage

- Computationally efficient
- Flexible model, physically based
- Keeps initial shape (topology)

## Snakes: disadvantages

- Requires initialization close to the final solution
- May converge to local minimum
- Quite dependent on tuning parameters (weighting internal and external forces)
- Numerical instability (may oscillate)
- Keeps initial shape (topology)

## Level set-based segmentation

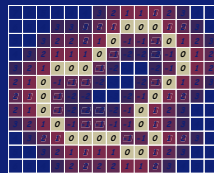
## Level sets: underlying idea

- Rather than evolving the curve/surface  $C(s)$ , embed the curve as a level set in a one-dimensional higher image:

▪ E.g. 
$$U(\vec{x}) = \pm d$$

where  $d$  is the distance to the  $C(s)$

- Evolve  $C(s)$  implicitly by evolving  $U(x)$



## Speed function

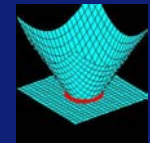
- Selected such that boundaries are captured
- Speed function only "makes sense" at the zero level set.
- Example speed function

$$g = \left[ \frac{1}{1 - |\nabla I|^2 / k^2} \right]$$

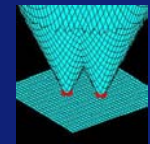
- Speed function can also be based on intensity, second order information, etc.

## Level sets: change in topology

- Curves and surfaces are represented as level sets in a higher dimensional function



- This has important advantages:
  - Topological changes can be handled naturally

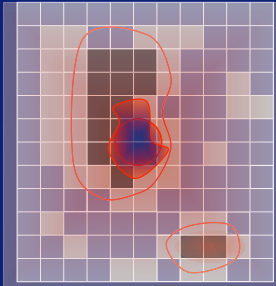




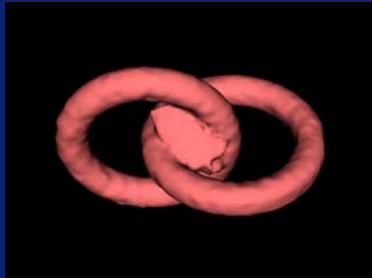
### Example level set evolution

Segmentation with LS:

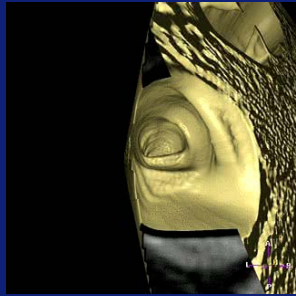
- Initialise the front  $C(0)$
- Compute  $u(x,y,0)$
- Iterate:
 
$$u(n+1) = u(n) + \Delta t g \|\nabla u\|$$
 until convergence
- Mark the front  $u(t_{end})$



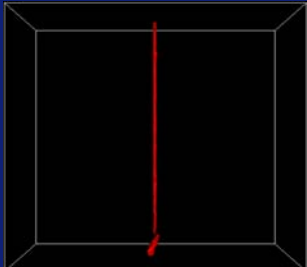
### 3D: Change of topology



### Applications



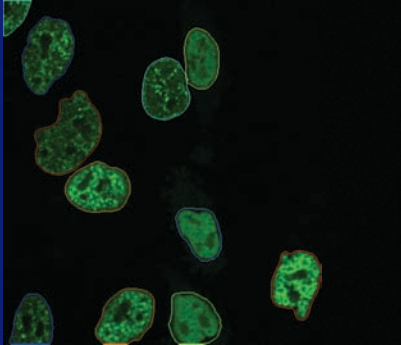
### Extension to vascular data

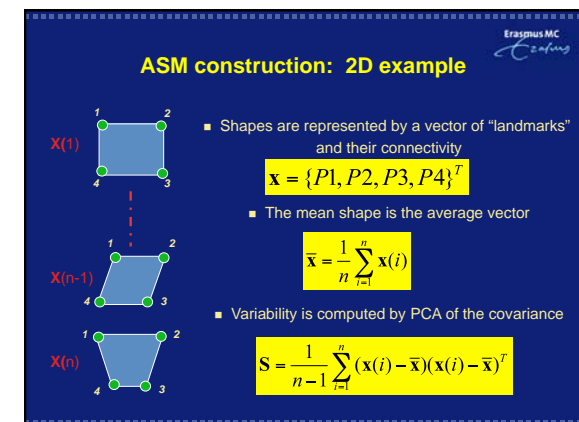
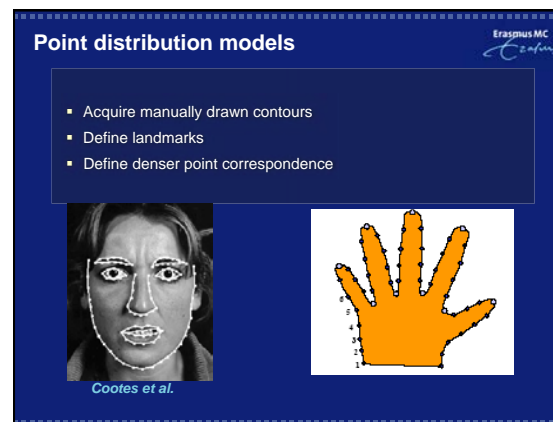
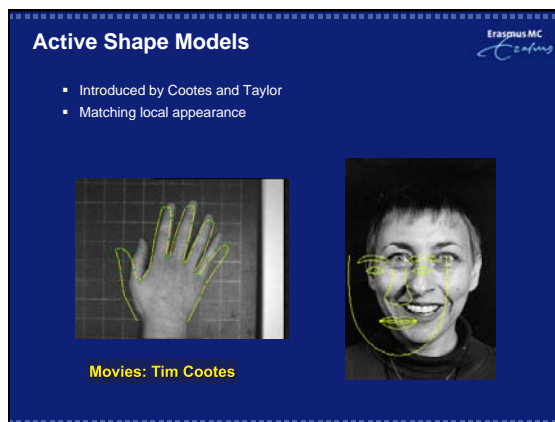
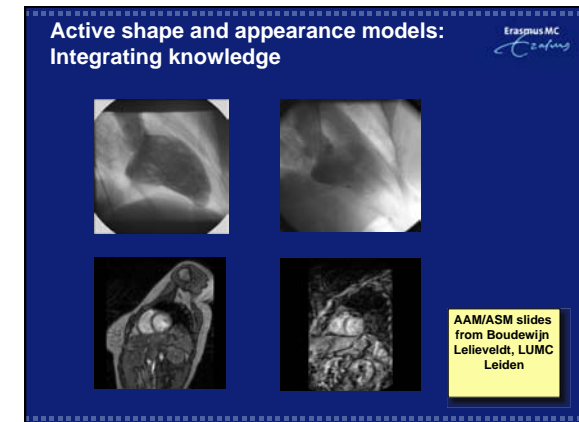
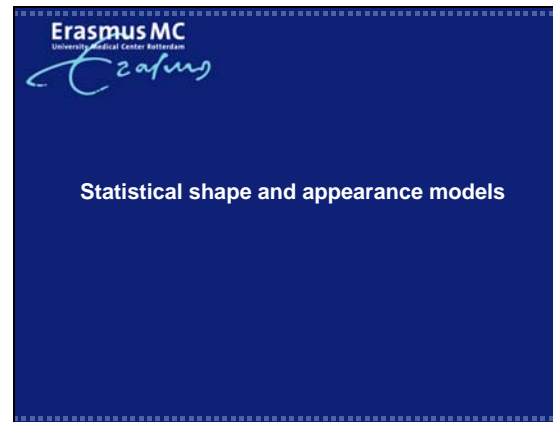
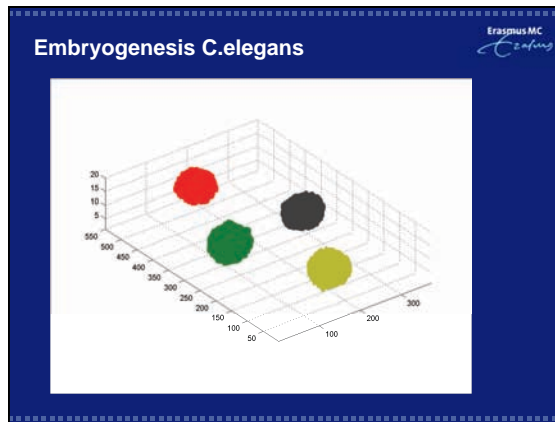


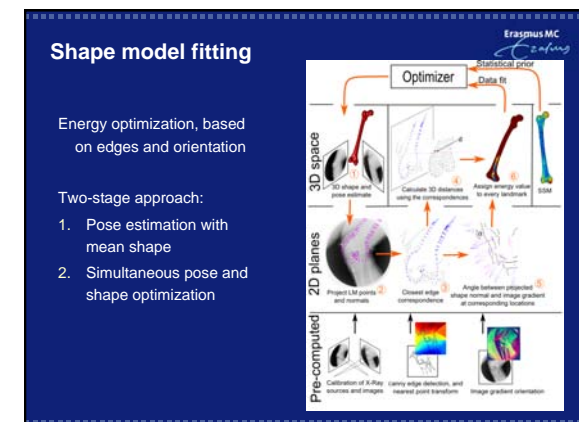
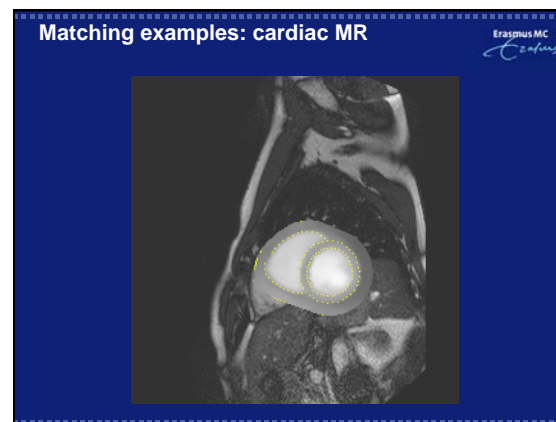
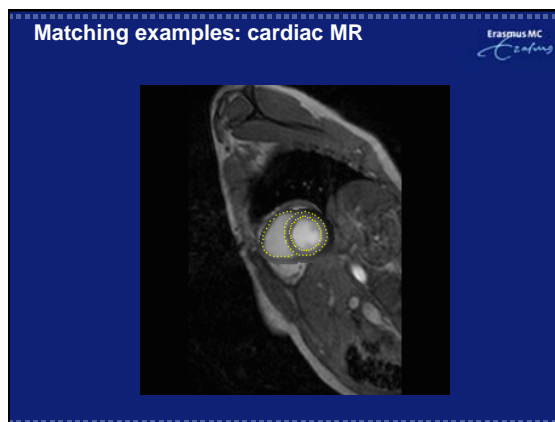
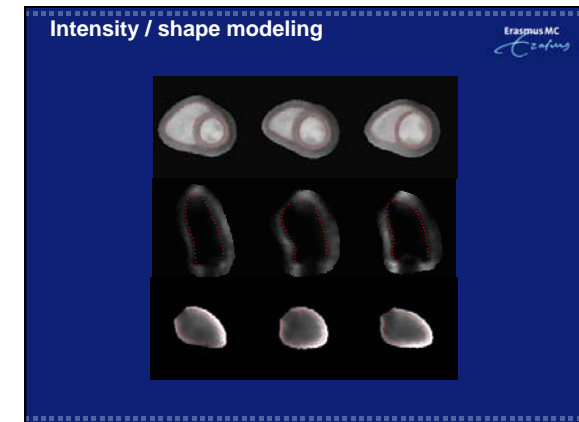
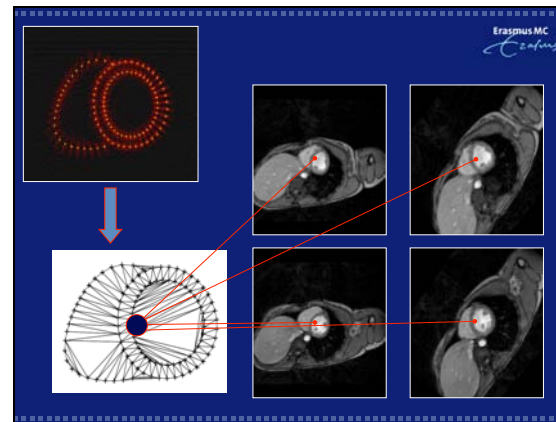
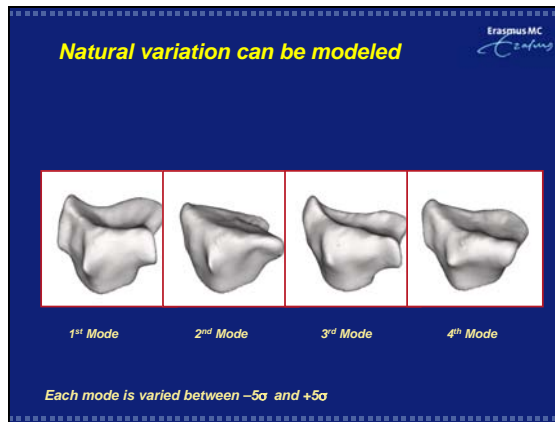
### Cell tracking examples



*Dzyubachyk et al. (2007)*



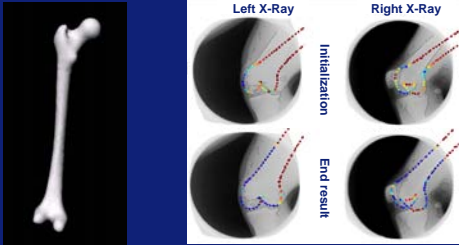




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### 3D shape reconstruction

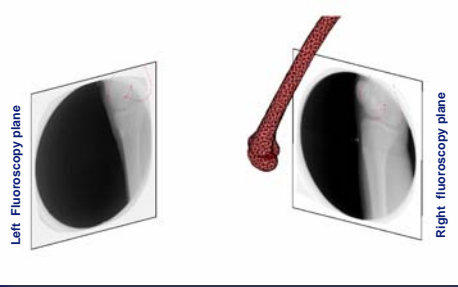
3D statistical shape model fitting to the Canny edge-map, and automatic selection of the relevant bony edges



The figure illustrates the 3D shape reconstruction process. On the left is a 3D model of a femur. On the right, four circular X-ray images are shown in a 2x2 grid. The top row is labeled 'Left X-Ray' and 'Right X-Ray'. The top-left image is labeled 'Initialization' and shows a red line representing the initial edge detection. The bottom-left image is labeled 'End result' and shows a blue line representing the final, refined edge detection. The top-right and bottom-right images show the corresponding edge detection for the right X-ray.

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### 3D femur reconstruction from biplane fluoroscopy



The figure shows the 3D femur reconstruction process. On the left, a 'Left Fluoroscopy plane' shows a 2D X-ray of a femur. On the right, a 'Right fluoroscopy plane' shows another 2D X-ray of the same femur. In the center, a 3D model of the femur is shown, with a red line representing the reconstructed 3D shape. The 3D model is positioned between the two fluoroscopy planes, demonstrating how the 3D shape is derived from the 2D images.

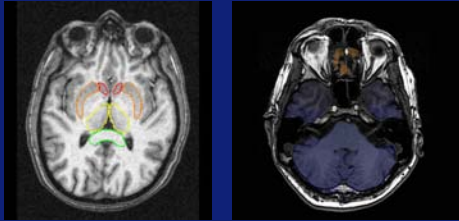
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### Atlas-based segmentation

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### Atlas-based segmentation of individual neurostructures

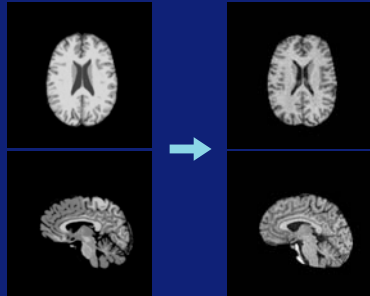
- Segmentation of multiple neurostructures



The figure shows two axial brain MRI slices. The left slice is labeled 'Labeled atlases' and shows various neurostructures highlighted in different colors (red, yellow, green, blue). The right slice is a standard axial brain MRI slice without labels.

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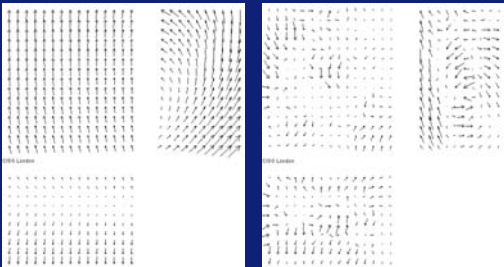
### Intersubject nonrigid registration



The figure illustrates intersubject nonrigid registration. It shows two sets of brain MRI slices: axial and sagittal. A blue arrow points from the left set of slices to the right set, indicating the registration process. The right set of slices shows the result of the nonrigid registration, where the slices are warped to match the shape of the slices in the left set.

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### Underlying deformation



The figure shows the underlying deformation of the brain MRI slices. It displays two sets of vector fields: 'Affine component' and 'Nonrigid component'. The 'Affine component' shows a regular grid of vectors, while the 'Nonrigid component' shows a more complex, irregular grid of vectors. The vectors represent the deformation of the brain MRI slices from the reference shape to the target shape.

